

Ber. nat.-med. Verein Innsbruck	Band 73	S. 215 – 220	Innsbruck, Okt. 1986
---------------------------------	---------	--------------	----------------------

## Comparison of the "theoretical" formula and a new formula for the calculation of intraocular lenses

by

Franz DAXECKER und Walter AMBACH \*)

(Univ.-Klinik für Augenheilkunde, Innsbruck, Vorstand: Univ.-Prof. Dr. W. Göttinger,  
Institut für Medizinische Physik, Innsbruck, Vorstand: Univ.-Prof. Dr. W. Ambach)

### Vergleich zwischen "theoretischer" Formel und einer neuen Formel bei der Berechnung der Brechkraft intraokularer Linsen

**Synopsis:** Zur Berechnung der Brechkraft intraokularer Linsen wird eine neue vereinfachte Formel vorgestellt, die mit Hilfe einer linearen TAYLOR-Reihe abgeleitet wird. Bei 140 Augen wird die Restrefraktion mit einer theoretischen Formel und mit der neuen Formel vorausberechnet und mit der tatsächlichen postoperativen Refraktion verglichen. Es zeigt sich, daß bei irisgetragenen Linsen die Vorausberechnung nach beiden Formeln gleich gute Ergebnisse bringt, bei Hinterkammerlinsen bringt die neue Formel bessere Ergebnisse.

#### Introduction:

Formulas for the calculation of the refracting power of intraocular lenses have been presented by various authors [1, 2, 3, 4]. These "theoretical" formulas appear almost identical when the appropriate mathematical transformation is applied. A new formula is presented in this paper derived from the formulas mentioned above using a linear TAYLOR-line. To prove the exactness of the calculation the results of the precalculations obtained with both formulas are compared with the post-operative residual refractions.

#### Methods of calculation and derivation of the new formula:

Formula A: Formula A based on the method described by GERNET [3] for the calculation of lens refraction. The refracting power of a natural and the artificial lens is described by WERNER [5] as follows:

$$D_L = \frac{n}{a-d} - \frac{n}{\frac{n}{D_C + D_B} - d} \quad (1)$$

\*) Anschrift der Verfasser: Doz. Dr. med. F. Daxecker, Univ.-Klinik für Augenheilkunde, Anichstraße 35, Univ.-Prof. Dr. phil. W. Ambach, Institut für Medizinische Physik, Müllerstraße 44, beide A-6020 Innsbruck, Österreich.

$D_L$  = Refracting power of the intraocular lens (D),  $a$  = Axial length of the eye (mm),  $d$  = Distance from the principal plane of the lens to the corneal vertex (mm),  $D_C$  = Refracting power of the cornea (D),  $D_B$  = Vertex power of spectacles (D),  $n$  = Refractive index of aqueous and vitreous (1.336),  $D$  = diopter.

The refracting power of the cornea is given as a result of:

$$D_C = \frac{n_H - n_L}{r} \quad (2)$$

$n_L$  = Refractive index of air (1.000),  $n_H$  = Refractive index of the cornea (1.332),  $r$  = Radius of curvature of the anterior surface of the cornea (mm). The remaining symbol as in formula (1).

For the calculation in mm you have to multiply  $n$ ,  $n_H$  and  $n_L$  with the factor 1000. For the calculation of the residual refraction, formula (1) is transformed into  $D_B$ .

Formula B:

a) Emmetropizing Lens:

With the use of a TAYLOR-line in a linear form [6] one obtains the following derivations from formula (1) ( $D_B = 0$ ):

$$\Delta D_L(a) = \frac{-1.336}{(a-d)^2} \cdot \Delta a \quad (3)$$

$$\Delta D_L(r) = \frac{+1.336 \cdot 4.024}{(4.024 r - d)^2} \cdot \Delta r \frac{n}{D_C} = 4.024 \quad (4)$$

$$\Delta D_L(d) = \frac{1.336}{(a-d)^2} - \frac{1.336}{(4.024 r - d)^2} \cdot \Delta d \quad (5)$$

The previously mentioned refractive indices are used.  $\Delta D_L(a)$ ,  $\Delta D_L(r)$  and  $\Delta D_L(d)$  correspond to a change of the refracting power of the lens when one single variable is altered.

With the use of the medians  $\bar{a} = 23.57$  mm,  $\bar{r} = 7.67$  mm,  $\bar{d} = 3.5$  mm [7, 8] the following are obtained from equations (3), (4) and (5):

$$\Delta D_L(a) = -3.31 \cdot \Delta a \quad (6)$$

$$\Delta D_L(r) = +7.18 \cdot \Delta r \quad (7)$$

$$\Delta D_L(d) = +1.53 \cdot \Delta d \quad (8)$$

$\Delta a$ ,  $\Delta r$  and  $\Delta d$  are to be in millimetres,  $\Delta D_L$  results in diopters. The median  $\bar{D}_L$  for an emmetropizing lens is 17.75 D. When the changes in refracting power [caused by single variables as shown in equations (6), (7) and (8)] are added, the result is

$$D_L = 17.75 + 3.31 (23.57 - a) - 7.18 (7.67 - r) - 1.53 (3.50 - d) \quad (9)$$

thus,

$$D_L = 35.34 - 3.31a + 7.18r + 1.53d \quad (10)$$

$$\Delta D_L(D_C) = \frac{-\frac{n^2}{D_C^2}}{\left(\frac{n}{D_C} - d\right)^2} \cdot \Delta D_C \quad (11)$$

With the use of the above mentioned medians one obtains ( $D_B = 0$ ):

$$\Delta D_L(D_C) = -1.27 \cdot \Delta D_C \quad (12)$$

and

$$D_L = 17.75 + 3.31 (23.57 - a) + 1.27 (43.28 - D_C) - 1.35 (3.5 - d) \quad (13)$$

thus,

$$D_L = 145.37 - 3.31a - 1.27 D_C + 1.35 d \quad (14)$$

The formula for the postoperative ametropia is formula (23) and for the residual refraction formula (25).

The refracting power of an emmetropizing lens can be calculated by using this formula (Fig. 1), see also the foot note\*).

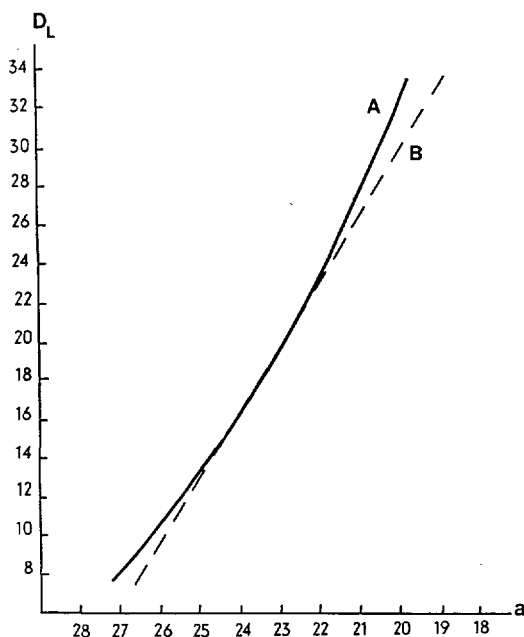


Fig. 1: Graph of the theoretical formula (A) and the new linear formula (B). Ordinate: lens power  $D_L$  in dipters, abscissa: axial length  $a$  in millimetres, refracting power of the cornea  $D_C$  is 43.28 D ( $r = 7.67$  mm) and the postoperative anterior chamber depth is 3.5 mm.

A simplification is possible:

The conversion factor from microseconds into millimetres for the time measured by ultrasound can be included in the equation (10). This factor 0.774 results from division of the axial acoustic velocity (1548 m/sec, [9]) and the conversion of seconds into microseconds and metres into millimetres.

\*) If the corneal radius is measured in diptres, the derivation has to be done after  $\Delta D_C$ .

The following results:

$$D_L = 35.34 - 2.56t + 7.18r + 1.53d \quad (16)$$

$$t = \mu\text{sec.}$$

b) Postoperative ametropia:

In the case of desired postoperative ametropia the procedure should be as follows and as shown in formula (1). The refracting power of spectacles is added to the refracting power of the cornea [3]. The connection between the radius of the cornea  $r$  and the refracting power of the cornea  $D_C$  is shown in formula (2). The refracting power of spectacles can also be expressed in a hypothetical change of the radius of the cornea [7].

The linear form of a TAYLOR-line can be derived from formula (2):

$$\Delta D_C = \frac{-n}{r^2} \cdot \Delta r \quad (17)$$

with the use of the median  $\bar{r} = 7.67$  mm one obtains

$$\Delta D_C = -5.6 \cdot \Delta r \quad (18)$$

Whereby  $\Delta D_C$  conforms to the emmetropizing spectacles  $D_B$  and procedure a change of the corneal radius:

$$\Delta r = \frac{D_B}{-5.6} \quad (19)$$

In order to determine the refracting power of the lens in desired postoperative ametropia it is necessary to add or subtract the quantity, that results from formula (19) to or from the measured radius in formula (10).

$$D_L = 35.34 - 3.31a + 7.18(r + \Delta r) + 1.53d \quad (20)$$

Formula (20) can be transformed to  $\Delta r$  and this results in:

$$-7.18\Delta r = [35.34 + 7.18r + 1.53d - 3.31a] - D_L \quad (21)$$

As can be seen in equation (21) the symbols in brackets in equation (10) conform to an emmetropizing lens from equation (10) is inserted instead of the parenthetical expression and equation (19) inserted instead of  $\Delta r$  in equation (21), the result is

$$1.28 D_{B \text{ (desired)}} = D_{L \text{ (emmetrop)}} - D_L \quad (22)$$

or

$$D_L = D_{L \text{ (emmetrop)}} - 1.28 \cdot D_{B \text{ (desired)}} \quad (23)$$

The emmetropizing lens will be called  $D_L$  (emmetrop) and the lens to be implanted will be called  $D_L$ ,  $D_B$  will be called  $D_{B \text{ (desired)}}$ .

c) Determination of the residual refraction on a given lens refraction:

When the calculated emmetropizing lens is not available or for some other reason a non-emmetropizing lens has to be implanted, a postoperativ residual refraction that can be precalculated appears.

There for formula (22) is transformed. The residual refraction is called  $D_{B \text{ (optional)}}$  and the non-emmetropizing lens is called  $D_{L \text{ (optional)}}$ .

$$D_B = \frac{D_{L(\text{emmetrop})} - D_{L(\text{optional})}}{1.28} \quad (24)$$

or as multiplication

$$D_B = [D_{L(\text{emmetrop})} - D_{L(\text{optional})}] \cdot 0.78 \quad (25)$$

i.e. the difference between an emmetropizing lens and a lens with a certain refracting power whose implantation is intended has to be multiplied by 0.78 to receive the prospective postoperative residual refraction.

## Patients:

In 70 eyes of iris supported lenses ( $d = 3.5$  mm) and 70 eyes of posterior chamber lenses ( $d = 4.0$  mm) the postoperative refraction is compared with the precalculated residual refraction. Measurement of the corneal radius was performed with the Zeiss-Ophthalmometer ( $n_H = 1.322$ ).

If there is astigmatism the median of the horizontal and vertical radius is used. For the measurement of the axial length the A-scan instrument 7200 MA (8 MHz) of Kretz technic is used. The following acoustic velocities are taken [9]:

Aqueous and vitreous 1532 m/sec., optic axis 1548 m/sec.

The preoperative residual refraction is calculated with formula (1) – A – and formula (25) – B.

In all cases postoperative vision is better than 0.5 and postoperative astigmatism less than 4 diopters. For the statistic calculation a minicomputer was established. The significances shown in the tables of Sachs [10] were used.

## Results:

The results are shown in the tables 1a und 1b.

Tables 1a, 1b: Comparison of the results of the preoperative calculated residual refraction by formula A and B and the actually postoperative residual refraction. n.s. = no significance.

residual refraction	correlation coefficient	probability	median (D)	standard deviation (D)
theoretical formula (A)	0.414	$p < 0.001$	−0.59	0.78
new formula (B)	0.447	$p < 0.001$	−0.56	0.79
postoperative refraction	—	—	−0.43	1.03

Table 1a: 70 patients with iris-supported lenses

residual refraction	correlation coefficient	probability	median (D)	standard deviation (D)
theoretical formula (A)	0.094	n.s.	−0.14	0.61
new formula (B)	0.264	$p < 0.5$	−0.27	0.62
postoperative refraction	—	—	−0.06	0.93

Table 1b: 70 patients with posterior chamber lenses

## Discussion:

We found, that there is no significant difference in the exactness of the precalculation with both formulas for the calculation of iris supported lenses. With both methods the correlation of pre- and

postoperative refraction is significant. This is not the case with posterior chamber lenses. There is no significant correlation using the theoretical formula for the calculation. Using the new formula there is a significant correlation between precalculation and postoperative refraction (Table 1a, 1b).

The new formula represents an easier method for the calculation of the refracting power of intraocular lenses. The formulas used for the calculation are formula (10) — or formula (14) for corneal refraction measured in diopters — for an emmetropizing lens, formula (25) for the residual refraction of the actually implanted lens, and formula (23) for the postoperative ametropia.

**Summary:** In order to calculate the refracting power of intraocular lenses a new formula is presented, which is derived from a theoretical formula, with the help of a TAYLOR-line. In 140 eyes the residual refractions are calculated with the help of a theoretical and the new formula. We can find that the results are the same in the case of iris supported lenses, but in the case of posterior chamber lenses better results have been achieved with the new formula.

## Literature:

1. BINKHORST, C.D. (1973): Dioptrienzahl künstlicher Augenlinsen. — *Klin. Mbl. Augenheilk.*, **162**: 629 - 634.
2. COLENBRANDER, M. (1973): Calculation of the power of an iris clip lens for distance vision. — *Brit. J. Ophthalm.*, **57**: 735 - 740.
3. GERNET, H., OSTHOLT, H. und WERNER, H. (1978): *Intraokulare Optik in Klinik und Praxis*. — Berlin, 168 pp.
4. BÜRKI, E. (1979): Zur Ermittlung des Dioptrienwertes der Binkhorst-Linse. — *Klin. Mbl. Augenheilk.*, **174**: 629 - 634.
5. WERNER, H., OSTHOLT, H. und GERNET, H. (1976): Beitrag zur augenseitigen Optik. — *Von Graefes Arch. Ophth.*, **199**: 281 - 299.
6. AMBACH, W. und F. DAXECKER (1983): Zur Berechnung der Brechkraftäquivalente optischer Größen des natürlichen Auges. — *Ber. nat.-med. Ver. Innsbruck*, **70**: 231 - 239.
7. DAXECKER, F. und W. AMBACH (1983): Nomogramm zur Bestimmung der Brechkraft intraokularer Linsen. — *Klin. Mbl. Augenheilk.*, **181**: 350 - 352.
8. DAXECKER, F. (1984): Neue Formeln zur Bestimmung der Brechkraft intraokularer Linsen. — *Klin. Mbl. Augenheilk.*, **184**: 208 - 210.
9. JANSSON, F. and E. KOCK (1963): Determination of the velocity of ultrasound in the human lens and vitreous. — *Acta Ophthal. Kbh.*, **40**: 420 - 430.
10. SACHS, L. (1969): *Statistische Auswertungsmethoden*. — 2. Aufl., Berlin—Heidelberg—New York, 415 pp.

# ZOBODAT - [www.zobodat.at](http://www.zobodat.at)

Zoologisch-Botanische Datenbank/Zoological-Botanical Database

Digitale Literatur/Digital Literature

Zeitschrift/Journal: [Berichte des naturwissenschaftlichen-medizinischen Verein Innsbruck](#)

Jahr/Year: 1986

Band/Volume: [73](#)

Autor(en)/Author(s): Daxecker Franz

Artikel/Article: [Comparison of the "theoretical" formula and a new formula for the calculation of intraocular lenses. 215-220](#)